



# **Optical probing depth in a wearable device: a Monte Carlo study**

#### **E. Esipenok**

N.I. Lobachevsky State University of Nizhny Novgorod

**M. Kirillin**

A.V. Gaponov-Grekhov Institute of Applied Physics of RAS

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### **Motivation**

- Wide employment of wearable devices with optical probing system for regular measurement of human physiological parameters
- Employment of optical diagnostic techniques to measure heart rate and blood oxygenation in wearable devices
- Assessing the probing depth when selecting the parameters of the measuring system for optimal device performance
- Impossibility to determine the probing depth in an experiment due to a requirement to place a detector inside the biological tissue



• Application of numerical modeling of signal formation in optical systems by the Monte Carlo technique allowing for tracing individual photon trajectories



Analysis of probing depth for configuration typical for wearable devices for probing wavelengths of 530, 655, and 940 nm using Monte Carlo technique. This approach allows to simultaneously obtain the dependence of tissue reflectance on source-detector distance and corresponding distribution of maximal probing depths that are reached by individual photon trajectories in the medium.

## Optical diffusion methods for studying biological tissue

Basic principle of optical diffusion spectroscopy Photon trajectory map calculated by

Monte Carlo technique





### Optical Methods in Wearable Devices

#### **Optical pulse measurement**



#### **Optical measurement of blood oxygenation**



Dual Wavelength Probing



Reconstruction of the oxygenation value



### Monte Carlo Technique



R: reflected photon A: absorbed photon T: transmitted photon

#### **Input parameters**

- $\mu_{\mathsf{s}}$  : scattering coefficient
- $\mu_{a}^{}$  : absorption coefficient
- *p*(*s*,*s'*) : scattering phase function
- *g*: anisotropy factor
- *n*: refractive index

# Optical properties of skin layers



 $n = 1.37; g = 0.9$ 

E. Sergeeva, D. Kurakina, I. Turchin, M.Yu. Kirillin, A refined analytical model for reconstruction problems in diffuse reflectance spectroscopy, *Journal of Innovative Optical Health Sciences,*   $2342002$  (2024).

OP: epidermis





Probing depth distributions versus source-detector distance



Physiological depths of the dermis: 0.3-1.5 mm (shown with beige strip)  $10^{10}$ 



Probing depth distributions for oxygenation measurements wavelengths

Similar distributions providing the same probing volume are achieved for *d* = 2.5 mm



Most probable probing depth *d* versus source detector distance *r*



- For the wavelength of 530 nm the range of the probing depth of 0.3 0.4 mm are achieved for the source-detector distances of 1 - 2 mm. Since blood absorption in the red and NIR ranges is smaller, the wavelengths from these ranges provide deeper probing.
- For the wavelength of 655 nm, the probing depth range of 0.3 1 mm is achieved for the source-detector distance of 1 - 4 mm, and the maximum proximity of the probing depth to the center of the dermis layer (0.8 - 1 mm) is achieved with a source-detector distance in the range: 2.5 - 4 mm.
- For the wavelength of 940 nm the probing depth range of 0.6 1.4 mm is achieved from the source-detector distance of 2 - 5 mm, with the maximum proximity of the probing depth to the center of the dermis layer (0.8 - 1 mm) for the source-detector distance in the range of 2.5-3.5 mm.
- For oxygenation measurements in wearable devices at wavelengths of 655 and 940 nm, the optimal source-detector distance is 2.5 mm for both wavelengths, providing the probing depth of 0.8 mm for wavelengths.



# Thanks for your attention!